World Journal of Gastrointestinal Surgery

World J Gastrointest Surg 2024 June 27; 16(6): 1485-1955





Published by Baishideng Publishing Group Inc

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Peer Reviewer of World Journal of Gastrointestinal Surgery, Deven Juneja, DNB, FNB, EDIC, FCCP, Director, Department of Critical Care Medicine, Max Super Speciality Hospital, New Delhi 110017, India. devenjuneja@gmail.com

AIMS AND SCOPE

The primary aim of World Journal of Gastrointestinal Surgery (WJGS, World J Gastrointest Surg) is to provide scholars and readers from various fields of gastrointestinal surgery with a platform to publish high-quality basic and clinical research articles and communicate their research findings online.

WJGS mainly publishes articles reporting research results and findings obtained in the field of gastrointestinal surgery and covering a wide range of topics including biliary tract surgical procedures, biliopancreatic diversion, colectomy, esophagectomy, esophagostomy, pancreas transplantation, and pancreatectomy, etc.

INDEXING/ABSTRACTING

The WJGS is now abstracted and indexed in Science Citation Index Expanded (SCIE, also known as SciSearch®), Current Contents/Clinical Medicine, Journal Citation Reports/Science Edition, PubMed, PubMed Central, Reference Citation Analysis, China Science and Technology Journal Database, and Superstar Journals Database. The 2024 Edition of Journal Citation Reports[®] cites the 2023 journal impact factor (JIF) for WJGS as 1.8; JIF without journal self cites: 1.7; 5-year JIF: 1.9; JIF Rank: 123/290 in surgery; JIF Quartile: Q2; and 5-year JIF Quartile: Q3.

RESPONSIBLE EDITORS FOR THIS ISSUE

Production Editor: Zi-Hang Xu; Production Department Director: Xiang Li; Cover Editor: Jia-Ru Fan.

| NAME OF JOURNAL | INSTRUCTIONS TO AUTHORS | | |
|---|---|--|--|
| World Journal of Gastrointestinal Surgery | https://www.wignet.com/bpg/gcrinfo/204 | | |
| ISSN | GUIDELINES FOR ETHICS DOCUMENTS | | |
| ISSN 1948-9366 (online) | https://www.wjgnet.com/bpg/GerInfo/287 | | |
| LAUNCH DATE | GUIDELINES FOR NON-NATIVE SPEAKERS OF ENGLISH | | |
| November 30, 2009 | https://www.wjgnet.com/bpg/gerinfo/240 | | |
| FREQUENCY | PUBLICATION ETHICS | | |
| Monthly | https://www.wjgnet.com/bpg/GerInfo/288 | | |
| EDITORS-IN-CHIEF | PUBLICATION MISCONDUCT | | |
| Peter Schemmer | https://www.wjgnet.com/bpg/gerinfo/208 | | |
| EDITORIAL BOARD MEMBERS | ARTICLE PROCESSING CHARGE | | |
| https://www.wjgnet.com/1948-9366/editorialboard.htm | https://www.wjgnet.com/bpg/gerinfo/242 | | |
| PUBLICATION DATE | STEPS FOR SUBMITTING MANUSCRIPTS | | |
| June 27, 2024 | https://www.wjgnet.com/bpg/GerInfo/239 | | |
| COPYRIGHT | ONLINE SUBMISSION | | |
| © 2024 Baishideng Publishing Group Inc | https://www.f6publishing.com | | |

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World Journal of Gastrointestinal Surgery

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World J Gastrointest Surg 2024 June 27; 16(6): 1571-1581

DOI: 10.4240/wjgs.v16.i6.1571

ISSN 1948-9366 (online)

ORIGINAL ARTICLE

Retrospective Cohort Study

Machine learning prediction model for gray-level co-occurrence matrix features of synchronous liver metastasis in colorectal cancer

Kai-Feng Yang, Sheng-Jie Li, Jun Xu, Yong-Bin Zheng

Specialty type: Surgery

Provenance and peer review:

Unsolicited article; Externally peer reviewed.

Peer-review model: Single blind

Peer-review report's classification Scientific Quality: Grade B, Grade C

Novelty: Grade B, Grade B Creativity or Innovation: Grade B, Grade B

Scientific Significance: Grade B, Grade B

P-Reviewer: Bordonaro M, United States; Wu J, China

Received: January 27, 2024 Revised: March 16, 2024 Accepted: April 25, 2024 Published online: June 27, 2024 Processing time: 154 Days and 20.1 Hours



Kai-Feng Yang, Yong-Bin Zheng, Department of Gastrointestinal Surgery, Renmin Hospital of Wuhan University, Wuhan 430030, Hubei Province, China

Sheng-Jie Li, Jun Xu, Department of Gastrointestinal Surgery, The First College of Clinical Medical Science, China Three Gorges University, Yichang Central People's Hospital, Yichang 443008, Hubei Province, China

Corresponding author: Yong-Bin Zheng, PhD, Doctor, Department of Gastrointestinal Surgery, Renmin Hospital of Wuhan University, No. 100 Zhangzhidong Road, Wuhan 430660, Hubei Province, China. yongbinzheng@whu.edu.cn

Abstract

BACKGROUND

Synchronous liver metastasis (SLM) is a significant contributor to morbidity in colorectal cancer (CRC). There are no effective predictive device integration algorithms to predict adverse SLM events during the diagnosis of CRC.

AIM

To explore the risk factors for SLM in CRC and construct a visual prediction model based on gray-level co-occurrence matrix (GLCM) features collected from magnetic resonance imaging (MRI).

METHODS

Our study retrospectively enrolled 392 patients with CRC from Yichang Central People's Hospital from January 2015 to May 2023. Patients were randomly divided into a training and validation group (3:7). The clinical parameters and GLCM features extracted from MRI were included as candidate variables. The prediction model was constructed using a generalized linear regression model, random forest model (RFM), and artificial neural network model. Receiver operating characteristic curves and decision curves were used to evaluate the prediction model.

RESULTS

Among the 392 patients, 48 had SLM (12.24%). We obtained fourteen GLCM imaging data for variable screening of SLM prediction models. Inverse difference, mean sum, sum entropy, sum variance, sum of squares, energy, and difference variance were listed as candidate variables, and the prediction efficiency (area under the curve) of the subsequent RFM in the training set and internal validation



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set was 0.917 [95% confidence interval (95% CI): 0.866-0.968] and 0.09 (95% CI: 0.858-0.960), respectively.

CONCLUSION

A predictive model combining GLCM image features with machine learning can predict SLM in CRC. This model can assist clinicians in making timely and personalized clinical decisions.

Key Words: Colorectal cancer; Synchronous liver metastasis; Gray-level co-occurrence matrix; Machine learning algorithm; Prediction model

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Core Tip: Our predictive model for synchronous liver metastasis (SLM) in colorectal cancer (CRC) patients can screen reliable predictive variables based on clinical features. This is crucial for predicting SLM in CRC and improving patient prognosis. Imaging omics is a discipline that has developed in recent years. Based on advanced deep learning algorithms, extracting imaging features will have practical clinical value for constructing prediction models for SLM in CRC. This study combines imaging and deep learning to construct an early warning prediction model, to provide necessary auxiliary predictions for the occurrence of SLM and guide clinical decision-making.

Citation: Yang KF, Li SJ, Xu J, Zheng YB. Machine learning prediction model for gray-level co-occurrence matrix features of synchronous liver metastasis in colorectal cancer. *World J Gastrointest Surg* 2024; 16(6): 1571-1581 URL: https://www.wjgnet.com/1948-9366/full/v16/i6/1571.htm DOI: https://dx.doi.org/10.4240/wjgs.v16.i6.1571

INTRODUCTION

Colorectal cancer (CRC), the third most common malignant tumor worldwide, has a high incidence and mortality rate[1]. Approximately 25%-30% of patients with CRC experience synchronous liver metastasis (SLM), and SLM is one of the most common causes of death in this disease[2,3]. However, despite advancements in surgical interventions, only about 25% of patients are suitable for resection surgery, which is considered a major curative treatment for SLM in CRC[4-6]. As such, early detection of SLM from CRC is important for diagnosis, treatment, and improvement of patient prognosis.

Deep learning algorithms use reliable algorithm development that integrates computing, storage, networking, and other technologies. Machine learning (ML) is a branch of artificial intelligence that focuses on predicting patterns in data through the use of mathematical algorithms. These algorithms are popular for accurately calculating and predicting cancer risk events by combining potential risk factors of tumor development[7]. Existing research has focused on the deep learning applications and integration of different data types to develop decision support tools. However, the lack of alternative candidate parameters for predicting disease urgently needs to be addressed. Imaging is a major component of cancer screening, staging, monitoring, and the evaluation of the aforementioned[8]. In this study, we extracted grayscale features from magnetic resonance imaging (MRI) images from patients with CRC and constructed a gray-level co-occurrence matrix (GLCM) to quantitatively measure texture characteristics.

We utilized GLCM features to capture texture information and image texture specificity to screen candidate variables and to establish a prediction model for SLM that helps clinicians make decisions and provides guidance for early clinical diagnosis and treatment decisions.

MATERIALS AND METHODS

Study population

We retrospectively selected 392 patients with CRC from the Gastrointestinal Surgery Department of Yichang Central People's Hospital from January 2015 to May 2023. The inclusion criteria were as follows: (1) Patients diagnosed with CRC and undergoing surgery; (2) patients aged \geq 18 years old; (3) patients with complete postoperative pathological information; (4) CRC is the only primary malignant tumor; and (5) patients undergoing preoperative MRI. The exclusion criteria included: (1) Patients who received neoadjuvant radiotherapy and chemotherapy before surgery; (2) patients with incomplete recorded baseline and pathological data; and (3) patients with positive surgical margins and distant metastasis other than SLM after tumor surgery. This retrospective study was approved by the Ethics Committee of Yichang Central People's Hospital, and the research protocol conforms to the accuracy of artificial intelligence model training while ensuring the confidentiality of personal privacy of all patients included in the study. The study received an informed consent exemption from the Ethics Committee. The process of incorporating patients and building prediction models is shown in Figure 1 and Supplementary Figure 1.

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Figure 1 The flow chart of patient selection and data process. SOS: Sum of squares; IND: Inverse difference; MES: Mean sum; SUV: Sum variance; SUE: Sum entropy; DIV: Difference variance; DIE: Difference entropy; RFM: Random forest model; ANNM: Artificial neural network model; GLRM: Generalized linear regression model; SLM: Synchronous liver metastasis.

Diagnostic criteria of SLM

Synchronous detection of liver metastasis was defined as SLM detected before or during the resection of the primary tumor, and in the case of unresectable patients, it was defined as SLM detected before or simultaneously with the primary tumor.

Acquisition of MRI-based radiomic parameters

We used Skyra 3.0T or Avanto 1.5T MRI instruments (provided by Siemens) to perform abdominal imaging examinations. The parameter settings were as follows: T2W1, TR 2500 ms, TE 83 ms, layer spacing 1.8 mm, layer thickness 6.0 mm, matrix 352 × 352, FOV 36 cm × 36 cm; The *b* values of DWI were set to 50 and 800, respectively. A vibe sequence was used for enhanced scanning, with TR 3.97 ms, TE 1.29 ms, and FOV 36 cm × 36 cm. Glucosamine gadolinium pentobate (*i.e.*, Magentavir, 0.2 mL/kg) was injected through the elbow vein at a rate of 2.0 mL/s, followed by 20.0 mL of physiological saline. We used an independent blind method to analyze the MRI images, including the maximum diameter of colorectal liver metastases (CRLM) before enhancement, the maximum diameter of CRLM during arterial phase, the edge of CRLM after enhancement, edge enhancement, and peripheral parenchymal enhancement.

Data entry and quality control analysis

To ensure the accuracy of data input, we used the following strategies. Firstly, the clinical baseline data and imaging data of patients were independently entered by two people, and the final analysis was proofread. Secondly, both imaging data and review were completed by two senior radiologists (with more than 7 years of experience). If there was a disagreement between the two during the film review, a third party made a ruling. Finally, all records included in this study had less than 5% missing data. Candidate variables exceeding this threshold were imputed using missing values (*i.e.*, median or mean imputation). If the missing value was greater than 10%, it was discarded immediately.

Training and verification of the segmentation model

We automatically extracted imageomics features (*i.e.*, T2W1 and VP images) from the VOIs of each patient's enhanced venous phase MRI image, including first-order features, morphological features, texture features, and filter-based higher-order features. These features were obtained by analyzing the original image and applying multiple filters to the derived images, including exponential filters, square filters, square root filters, logarithmic filters, and wavelet decomposition. Image texture features (*i.e.*, exponent, square, square root, logarithm, and wavelet transform) were divided into three subgroups: GLCM, including the sum of squares (SOS), mean sum (MES), the inverse difference (IND), sum entropy (SUE), correlation, sum variance (SUV), difference entropy (DIE), difference variance (DIV), energy, entropy, and contrast, grayscale length matrix, and grayscale shape matrix. In addition, wavelet decomposition included three-dimensional wavelet transform with low-pass filtering and high-pass filtering to quantitatively capture MRI image features.

We adopted a random grouping method (70% and 30% were included in the training and internal validation sets, respectively). In addition, we use lasso regression (*i.e.*, with minimum penalty coefficient and Pearson correlation coefficient) to select candidate predictive variables to use to construct SLM prediction models. We used three popular ML algorithms, namely the generalized linear regression model (GLRM), random forest model (RFM), and artificial neural

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network model (ANNM), to construct a visual prediction model for SLM[9-12]. We chose the minimum absolute shrinkage and selection operator algorithm and then constructed an SLM prediction model based on MRI features^[13]. We used decision curve analysis (DCA)[14], receiver operating characteristic (ROC), and clinical impact curves (CIC) to evaluate the predictive performance of each predictive model[15].

Statistical analysis

The categorical variables and continuous variables involved in this statistical analysis were tested using the chi-square test, Wilcoxon rank sum test, or T-test, respectively. As for the correlation analysis between two continuous variables, we used the Pearson correlation coefficient evaluation [16]. We used R studio software for data visualization and statistical analysis. A P value less than 0.05 was considered statistically significant.

RESULTS

Comparison of clinical characteristics between SLM and non-SLM groups

In the study, a total of 392 patients with CRC were included for SLM prediction model construction. Among them, 48 and 344 patients were assigned to the SLM group and non-SLM group, respectively. The incidence of SLM in the training and validation sets was 13.87% (38/274) and 8.47% (10/118), respectively. The baseline data of the two groups of patients with CRC are summarized in Table 1 and Supplementary Table 1.

Selection of candidate variables for constructing SLM prediction models

Considering that the candidate variables have biases and non-normal distributions, we performed loss function correction (i.e., added penalty coefficients) to facilitate the selection of the optimal variables. By setting penalty coefficients, we ensured that the coefficients of features with smaller impacts will be infinitely close to zero [i.e., least absolute shrinkage and selection operator (LASSO) regression coefficient screening] to ensure that important features are retained. In the subsequent prediction model construction, we selected candidate variables from 21 variables based on the LASSO coefficient curve to construct independent variables for predicting the risk of SLM. The independent variables were tumor type, vascular invasion, energy, SOS, IND, MES, SUV, SUE, and DIV (Figure 2).

Construction of SLM nomogram prediction model

We conducted a logistic regression analysis on all candidate variables (Supplementary Table 2) and ultimately established 9 variables as independent risk predictors for SLM. Based on the Akaike information criterion, we then established a prediction model for SLM and drew a nomogram (Figure 3; Supplementary Table 2). Finally, with the help of nomogram visualization analysis, we evaluated the specific risk coefficient of SLM in patients based on the corresponding risk scale values of the total score. In addition, the C-index value, validated internally by the bootstrap method, was 0.739, indicating that the predictive model had good clinical robustness.

Construction of the ML-based SLM prediction model

RFM and ANNM are the most commonly used algorithms in ML[9]. In this study, we established SLM prediction models based on four ML algorithms. As shown in Supplementary Table 3, in the RFM prediction model, IND, MES, SUE, DIV, SOS energy, and SUV were the top-ranking weight values, indicating that these variables are potential candidate variables for RFM prediction of SLM (Figure 4). Meanwhile, ANNM, IND, MES, SUE, DIV, SOS energy, and SUV were candidate variables to predict SLM, and their weight proportions in the three different algorithm prediction models did not match, highlighting the different prediction weights of candidate variables (Figure 5; Supplementary Table 4).

Performance of SLM prediction models

The ROC curve showed that the predictive efficacy of RFM in predicting SLM in the training and validation sets was area under the curve (AUC): 0.917 [95% confidence interval (95%CI): 0.866-0.680] and AUC: 0.09 (95%CI: 0.858-0.960), respectively. The ROC curve of ANNM in predicting SLM in the training and validation sets was AUC: 0.796 (95%CI: 0.745-0.847) and AUC: 0.806 (95%CI: 0.755-0.857), respectively, indicating that the predictive efficacy was not as good as RFM. Table 2 and Supplementary Figure 2 show the predictive performance of preoperative GLCM-based radiomics for SLM. Overall, the predictive efficiency of the SLM models based on ML algorithms for patients with CRC is significantly better than GLRM.

In Figure 6, the horizontal and vertical axes of DCA represent the threshold probability and net benefit, respectively. The black horizontal line indicated that when all patients had no SLM status, the net benefit rate was zero. Conversely, the gray diagonal line indicated the gap between all SLM patients receiving treatment and their ideal state. The DCA curve can assist in guiding the clinical performance of predictive models, thereby evaluating the superiority or inferiority of these models.

Performance evaluation of SLM prediction model based on ML

To further evaluate the discriminative efficiency of the RFM prediction models, we used CIC. As shown in Supplementary Figure 3, RFM can distinguish SLM patients and was highly consistent with the postoperative pathological examination results. Our research indicates that RFM, as a predictive tool for evaluating SLM in patients with CRC, has high predictive reliability and may be used as a clinical decision aid. This also shows that RFM is more suitable for



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| Table 1 Clinicopathological characteristics of patients with colorectal cancer, n (%) | | | |
|---|---------------------------|--|--|
| Variables | Overall (<i>n</i> = 392) | | |
| Age, yr | | | |
| ≥ 60 | 215 (54.8) | | |
| < 60 | 177 (45.2) | | |
| Sex | | | |
| Male | 194 (49.5) | | |
| Female | 198 (50.5) | | |
| BMI, kg/m ² | | | |
| ≤18.5 | 101 (25.8) | | |
| 18.5-23.9 | 89 (22.7) | | |
| 24.0-27.9 | 104 (26.5) | | |
| ≥ 28.0 | 98 (25.0) | | |
| Smoking | | | |
| Yes | 201 (51.3) | | |
| No | 191 (48.7) | | |
| Drinking | | | |
| Yes | 222 (56.6) | | |
| No | 170 (43.4) | | |
| Intestinal polyp | | | |
| Yes | 180 (45.9) | | |
| No | 212 (54.1) | | |
| AST, U/L | | | |
| < 40 | 203 (51.8) | | |
| ≥ 40 | 189 (48.2) | | |
| ALT, U/L | | | |
| < 50 | 179 (45.7) | | |
| ≥ 50 | 213 (54.3) | | |
| Hypertension | | | |
| Yes | 180 (45.9) | | |
| No | 212 (54.1) | | |
| Diabetes | | | |
| Yes | 183 (46.7) | | |
| No | 209 (53.3) | | |
| CEA, ng/mL | | | |
| Normal | 216 (55.1) | | |
| Abnormal | 176 (44.9) | | |
| CA199, U/mL | | | |
| Normal | 194 (49.5) | | |
| Abnormal | 198 (50.5) | | |
| AFP, ng/mL | | | |
| ≤100 | 191 (48.7) | | |
| > 100 | 201 (51.3) | | |



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| HbsAg | | | |
|---------------------------|-------------------------|--|--|
| Yes | 203 (51.8) | | |
| No | 189 (48.2) | | |
| Tumor type | | | |
| Adenocarcinoma | 211 (53.8) | | |
| Mucinous adenocarcinoma | 181 (46.2) | | |
| Tumor size, cm | | | |
| < 5 | 204 (52.0) | | |
| ≥5 | 188 (48.0) | | |
| NI | | | |
| Yes | 180 (45.9) | | |
| No | 212 (54.1) | | |
| VI | | | |
| Yes | 134 (34.2) | | |
| No | 258 (65.8) | | |
| Energy, median [IQR] | 3.91 [2.55, 5.62] | | |
| SOS, median [IQR] | 0.88 [0.69, 1.05] | | |
| IND, median [IQR] | 1.46 [1.17, 1.80] | | |
| MES, median [IQR] | 2.84 [1.94, 3.36] | | |
| SUV, median [IQR] | 20.90 [16.28, 25.33] | | |
| SUE, median [IQR] | 22.20 [17.10, 27.10] | | |
| DIV, median [IQR] | 87.50 [67.00, 107.00] | | |
| Contrast, median [IQR] | 291.00 [275.00, 308.00] | | |
| Correlation, median [IQR] | 16.13 [12.00, 19.22] | | |
| Entropy, median [IQR] | 2.17 [1.62, 2.64] | | |
| DIE, median [IQR] | 230.00 [188.00, 276.00] | | |

IQR: Inter-quartile range; BMI: Body mass index; AST: Aspartate aminotransferase; ALT: Alanine aminotransferase; CEA: Carcinoembryonic antigen; CA199: Carbohydrate antigen199; AFP: Alpha-fetoprotein; NI: Neural infiltration; VI: Vascular invasion; SOS: Sum of squares; IND: Inverse difference; MES: Mean sum; SUV: Sum variance; SUE: Sum entropy; DIV: Difference variance; DIE: Difference entropy; HbsAg; Hepatitis B surface antigen.

| Table 2 Comparison of predictive efficacy of pulmonary infection prediction models via receiver operating characteristic curves | | | | | | |
|---|--------------|-------------|------------------------|-------------------------|-------------|------------------------|
| Madal | Training set | | | Internal validation set | | |
| Woder | AUC mean | AUC 95%CI | Variables ¹ | AUC mean | AUC 95%CI | Variables ¹ |
| RFM | 0.917 | 0.866-0.968 | 7 | 0.909 | 0.858-0.960 | 7 |
| ANNM | 0.796 | 0.745-0.847 | 7 | 0.806 | 0.755-0.857 | 7 |
| GLRM | 0.783 | 0.732-0.834 | 6 | 0.739 | 0.688-0.790 | 6 |

¹Variables included in the model.

RFM: Random forest model; GLRM: Generalized linear regression model; AUC: Area under the curve; 95% CI: 95% confidence interval; ANNM: Artificial neural network model.

preoperative risk assessment in SLM.



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Figure 2 Predictor variable selection based on the least absolute shrinkage and selection operator regression method. A: Optimal parameter (lambda) selection in the least absolute shrinkage and selection operator (LASSO) model; B: LASSO coefficient profiles of the candidate features.



Figure 3 Nomogram prediction model for predicting synchronous liver metastasis in patients with colorectal cancer. A: Nomogram predicts risk of synchronous liver metastasis; B: The calibration curves for the nomogram. IND: Inverse difference; SUE: Sum entropy; DIV: Difference variance; SOS: Sum of squares; SUV: Sum variance.

DISCUSSION

CRC is one of the main contributors to global cancer incidence and mortality. Distant metastasis is the predominant reason for poor patient prognosis and the liver is the most common metastatic organ[17,18]. Previous studies have shown that the survival rate of patients with regional or distal CRC is low, and if there is no metastasis, the prognosis is better[2, 19]. Over 25% of patients with CRC have SLM detected at the first diagnosis, and up to 25% have SLM detected after



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Figure 4 Construction of synchronous liver metastasis prediction model via random forest model. A: The application prediction model formula of random forest model (RFM) is as follows: C = argmax (Σ (Ci)), where "Ci" represents the type of in prediction for the i-th tree, "C" is the final classification result, and "I" is the number of trees; B: The gravel plot indicates the robustness of the RFM prediction model. IND: Inverse difference; MES: Mean sum; SUV: Sum variance; SUE: Sum entropy; DIV: Difference variance; DIE: Difference entropy; RFM: Random forest model; ANNM: Artificial neural network model; GLRM: Generalized linear regression model; SLM: Synchronous liver metastasis; BMI: Body mass index; AST: Aspartate aminotransferase; ALT: Alanine aminotransferase; CEA: Carcinoembryonic antigen; CA199: Carbohydrate antigen 199; AFP: Alpha-fetoprotein; NI: Neural infiltration; VI: Vascular invasion; HbsAg: Hepatitis B surface antigen

primary tumor resection [20-22]. More than one-third of patients with CRC already have cancer development into all liver tissues when SLM is diagnosed[23]. Early detection can lead to early treatment and reduce mortality. Thus, effective SLM biomarkers may contribute to early treatment management. In this study, we constructed a GLCM composed of MRI, which has the potential to evaluate SLM in CRC patients based on feature-based risk scoring. We found that indicates that preoperative MRI examination and texture analysis using sequence images in CRC have significant application prospects in the risk stratification of SLM.

Although radiomic models have been increasingly used in computer-aided diagnosis and imaging biomarkers, their application in computed tomography or MRI is limited by the variability of image characteristics generated by different scanners, imaging protocols, patient anatomies, and increasingly diverse reconstruction and post-processing software[24, 25]. While these effects can be mitigated through careful data management and protocol standardization, these measures are impractical for applying to different sources of image data. In this study, we adopted a generalized traditional end-toend imaging system model, using radiomic calculations as an explicit stage[26]. This model not only predicts unexpected variability in radiomics but also forms an estimation of the true potential of radiomics. This framework has the potential to standardize radiomics under imaging conditions, making radiomics more widely applicable. We added candidate variables with predicted values to the ML-based algorithm model, and the results showed that the GLCM-based prediction efficiency reaches the highest of 0.917 without distinguishing the predicted variables.

ML can handle complex phenomena through data-driven analysis^[27]. Compared with traditional methods, ML significantly reduces the prediction error of trajectories [28,29]. Consistent with previous studies, this study also indicates that due to the continuous updating of predictive model algorithms, ML models typically provide better predictive

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Figure 5 Construction of pulmonary infection prediction model *via* **artificial neural network model.** A: The formula of artificial neural network model is as follows: $\theta = \theta \cdot \eta \times \nabla$ (θ). J (θ). Among them " η " is the learning rate, "so (θ). J (θ)" represents the gradient change of the loss function [*i.e.*, J(θ)]; B: Variable importance using connection weights for the artificial neural network model. IND: Inverse difference; SUV: Sum variance; SUE: Sum entropy; DIV: Difference variance; SOS: Sum of squares; MES: Mean sum.



Figure 6 Prediction performance of synchronous liver metastasis risk based on different supervised algorithm. A: Decision curve analysis (DCA) for three prediction models in the training set; B: DCA for three prediction models in the testing set. RFM: Random forest model; ANNM: Artificial neural network model; GLRM: Generalized linear regression model.

performance than traditional linear models[30]. These models can effectively utilize limited data and improve the robustness of prediction models by transferring existing similar models or training them repeatedly. For example, the best prediction model trained in this study, RFM, had superior robustness and prediction accuracy compared to traditional linear regression models. These results further confirm the generalizability and clinical applicability of deep learning in combining radiomics to predict synchronous SLM.

This study has some limitations. Firstly, due to the standard requirements of the acquisition of MRI parameters and equipment, the sample size included in this study is relatively small and comes from a single center. Future prospective cohort studies encompassing multiple centers and large samples should be conducted. Secondly, as a retrospective study, there is inevitably selection bias in the inclusion of research subjects, as well as potential bias caused by personal experience or non-objective factors. Thirdly, this study obtained GLCM-related parameters based on MRI but did not include features such as high-order textures in the analysis. Therefore, it is necessary to optimize and expand the filtering of high-order texture parameters in subsequent research, to obtain more candidate variables with potential predictive value to construct better SLM prediction models.

CONCLUSION

Combining ML-based algorithms with readily available GLCM radiomic features can quickly and accurately assess the risk of SLM in patients with CRC before surgery. In particular, algorithms based on RFM can help clinicians identify high-risk patients with SLM promptly, and make robust surgical decisions.

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FOOTNOTES

Author contributions: Zheng YB is responsible for the conceptualization and design of this project; Yang KF and Zheng YB are responsible for manuscript writing and monitoring the progress of the project; Li SJ and Xu J are responsible for data collection, analysis, and visualization; and all authors shall verify and submit the manuscript.

Institutional review board statement: The study was reviewed and approved by the Institutional review board of Yichang Central People's Hospital (Approval No. 2023-089-01).

Informed consent statement: As the study only involved retrospective chart reviews, informed written consents were not required in accordance with institutional IRB policy.

Conflict-of-interest statement: The authors declare that they have no conflict of interest to disclose.

Data sharing statement: No additional data are available.

STROBE statement: The authors have read the STROBE Statement – checklist of items, and the manuscript was prepared and revised according to the STROBE Statement-checklist of items.

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Country of origin: China

ORCID number: Yong-Bin Zheng 0009-0008-4452-446X.

S-Editor: Chen YL L-Editor: A P-Editor: Zhang XD

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