

Left atrial physiology and pathophysiology: Role of deformation imaging

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Abstract

The left atrium (LA) acts as a modulator of left ventricular (LV) filling. Although there is considerable evidence to support the use of LA maximum and minimum volumes for disease prediction, theoretical considerations and a growing body of literature suggest to focus on the quantification of the three basic LA functions: (1) Reservoir function: collection of pulmonary venous return during LV systole; (2) Conduit function: passage of blood to the left ventricle during early LV diastole; and (3) Contractile booster pump function (augmentation of ventricular filling during late LV diastole). Tremendous advances in our ability to non-invasively characterize all three elements of atrial function include speckle tracking echocardiography (STE), and more recently cardiovascular magnetic resonance myocardial feature tracking (CMR-FT). Corresponding imaging biomarkers are increasingly recognized to have incremental roles in determining prognosis and risk stratification in cardiac dysfunction of different origins. The current editorial introduces the role of STE and CMR-FT for the functional assessment of LA deformation as determined by strain and strain rate imaging and provides an outlook of how this exciting field may develop in the future.

Key words: Left atrium; Strain; Strain rate; Physiology; Pathophysiology; Cardiovascular magnetic resonance; Echocardiography; Feature tracking; Speckle tracking; Diastolic dysfunction

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Core tip: Recent advances in speckle tracking echocardiography (STE) and cardiovascular magnetic resonance myocardial feature tracking (CMR-FT) allow a detailed quantification of left atrium (LA) dynamics in terms of strain and strain rate imaging. Corresponding imaging biomarkers are progressively found to have the potential to predict the outcome in a variety of cardiovascular disease states. The current editorial introduces the role of STE and CMR-FT for the functional assessment of LA deformation and provides an outlook of how this exciting field may evolve in the future.

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INTRODUCTION

Heart failure of different origins including ischemic aetiology remains a major determinant of mortality^[1]. Left atrial (LA) enlargement has been shown to be a sensitive parameter for the prediction of adverse cardiac events^[2,3]. The interplay between LA enlargement and atrial remodelling in the development of atrial fibrillation (AF) has been demonstrated^[4,5]. However, the pure relation of LA pathology to its enlargement within different diseases may oversimplify cardiovascular physiology. It is important to note that the LA does not merely represent a stiff chamber, which passively transports blood from the pulmonary veins to the left ventricle (LV), but a more complex and active chamber. Its role should rather be described as a dynamic modulation of LV filling by functioning as a reservoir, conduit and contractile booster pump^[6,7]. There have been tremendous advances in terms of our ability to characterize all three elements of atrial function using non-invasive imaging techniques^[8]. Recent advances include LA deformation analysis using speckle tracking echocardiography (STE)^[9,10] as well as cardiovascular magnetic resonance myocardial feature tracking (CMR-FT)^[7,11]. Corresponding imaging biomarkers are progressively found to have the potential to predict the outcome in a variety of cardiovascular disease states^[6]. The current editorial introduces the role of STE and CMR-FT for the quantification of LA dynamics as expressed by strain and strain rate (SR) imaging and provides an outlook of how this exciting field may evolve in the future.

LA DEFORMATION ANALYSIS

Besides conventional techniques to analyse LA func-

tional parameters (e.g., pulmonary venous velocity, LA phasic volumes, mitral valve inflow velocity or mitral annular velocity; recent advances in deformation analysis allow to quantify LA longitudinal strain and SR using STE or - more recently - CMR-FT^[7,11] (Figure 1). Strain and SR represent the magnitude and rate of myocardial deformation (please see the review by Gorcsan and Tanaka for in depth explanation^[12]). LA strain profiles result in three aspects of LA physiology: passive strain (ϵ_E , representing LA conduit function), active strain (ϵ_A , representing LA contractile booster pump function) and total strain (ϵ_S , representing atrial reservoir function)^[7] (Figure 1 and Table 1). Correspondingly, three SR parameters can be quantified: peak positive strain rate (SR_S, representing LA reservoir function), peak early negative strain rate (SR_E, representing LA conduit function) and peak late negative strain rate (SR_A, representing LA contractile booster pump function)^[7] (Figure 1 and Table 1). It is interesting to speculate on the physiological relevance of the three LA functional elements: LA reservoir function as a measure of LA compliance and LA active relaxation may represent a compensatory mechanism at early stages of congestive LV failure. Conversely, LA conduit function as a measure of LA compliance is already affected by early diastolic LV relaxation abnormalities with changes in LV stiffness and compliance. Lastly LA booster pump function representing LA contractility has impact on ventricular filling and cardiac output^[13].

LA deformation quantification comprises challenges that are not present when dealing with ventricular strain and SR imaging. These include the insertion of pulmonary veins and the presence of the LA appendage, the thin LA wall and the variable LA geometry^[7]. Notwithstanding these facts, 2D STE and CMR-FT have both shown good performance and reproducibility of LA deformation analysis^[7,14]. However, using two-dimensional representations of 3D structures may oversimplify the complex LA anatomy. Through-plane motion or reduced STE imaging quality with poor imaging windows can affect LA deformation analysis and may be difficult to correct. Recent advances in STE provide three-dimensional imaging that eliminates the effects of through-plane motion in patients with sufficient imaging windows and may allow the comprehensive analysis of global and regional LA strain^[15,16]. At the present time, similar developments for CMR-FT based on three-dimensional imaging have not yet been introduced.

STE

Two-dimensional STE makes use of offline software analysis using conventional gray scale B-mode images, which are typically acquired during a breath-hold. The frame rate is set between 50 and 70 frames/sec. Speckles can be described as acoustic markers distributed within the myocardium, which can be

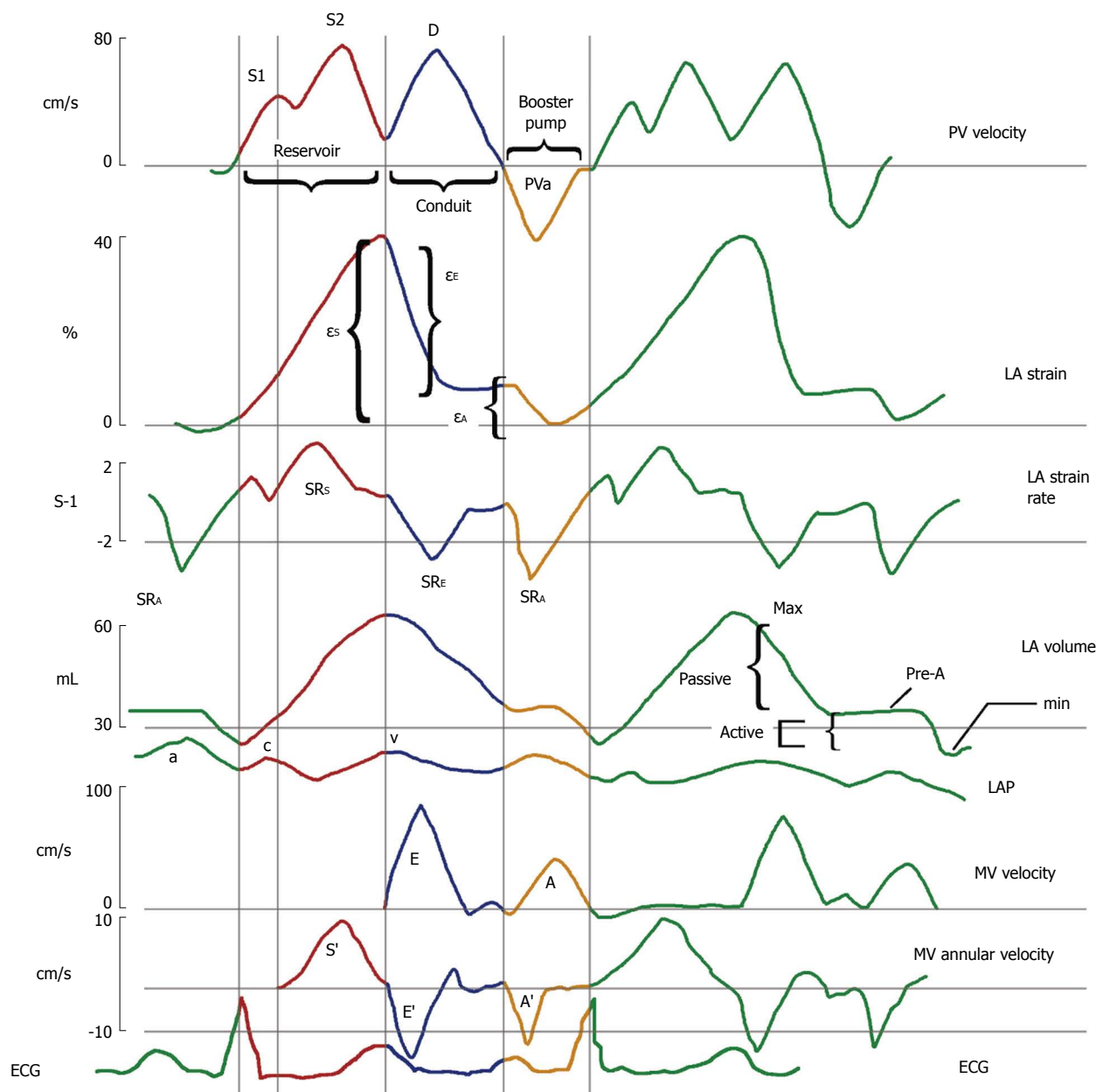


Figure 1 Left atrial physiology imaging using different methods. The figure displays pulmonary venous (PV) velocity, left atrial (LA) strain (ϵ), LA strain rate (SR), LA volume, left atrial pressure (LAP), and mitral spectral and tissue Doppler. Displayed are two cardiac cycles and the color-coded imaging of reservoir, conduit, and booster pump functions in red, blue, and yellow lines are shown within the first cardiac cycle, respectively. Reprinted from *Journal of the American College of Cardiology*, Vol 63, Brian D. Hoit, Left atrial size and function: role in prognosis, 493-505, 2014 with permission from Elsevier^[6].

tracked from frame to frame^[17]. This provides local myocardial displacement information, which can be utilized for the calculation of velocity, strain or SR. It is important to note that there is currently a lack of standardization for LA STE resulting in different approaches to calculate LA deformation indexes: LA strain and SR have been calculated by averaging values from a 15-segment model^[18] (six equidistant segments in the apical 4-chamber view, six in the 2-chamber view and three in the 3-chamber view) or from a 12-segment model^[14] (six equidistant segments in the 4-chamber view and six segments in the 2-chamber view). Usually, strain and SR indexes

are averaged from a total of three consecutive cardiac cycles that provide stable electrocardiographic recording. Furthermore, it is important to understand that there are two different approaches to quantify LA strain with STE. Based on the reference point set at the onset of the P wave (corresponding to the beginning of the atrial cycle)^[10,19] or set at the QRS-complex (corresponding to the beginning of the ventricular cycle)^[14,20], different LA strain profiles are generated. The description above and the explanation in Figure 1 represent strain profiles acquired with the reference point set at the onset of the QRS-complex resulting in the acquisition of reservoir, conduit and booster pump

Table 1 Left atrial strain and strain rate indexes as determined by speckle tracking echocardiography and cardiovascular magnetic resonance myocardial feature tracking

LA function	Strain	Strain rate
Reservoir	ϵ_S	SR _S
Conduit	ϵ_E	SR _E
Booster pump	ϵ_A	SR _A

Nomenclature refers to the QRS complex set as the reference point and is therefore applicable to both speckle tracking echocardiography and cardiovascular magnetic resonance myocardial feature tracking. LA: Left atrial; ϵ : Strain; SR: Strain rate.

function^[6]. In contrast, if the reference point is set at the onset of the P wave, LA strain profiles display early negative strain (representing LA booster pump function) followed by peak positive strain (representing LA conduit function) while their sum corresponds to LA reservoir function^[6].

The wide availability and high temporal resolution of echocardiographic real time images are advantages of STE. However, due to the far-field location of the LA, the main drawback of STE is its dependency on high quality images that frequently cannot be guaranteed in patients with limited acoustic windows^[14].

CMR-FT

CMR-FT allows tracking of tissue voxel motion directly from standard steady-state free precession (SSFP) cine CMR images and derivation of myocardial deformation (Figure 2) without the need for additional sequence acquisition as compared to myocardial MR Tagging^[7]. Therefore, this technique appears particularly applicable from a clinical perspective and can be easily implemented into a running CMR laboratory. Although CMR-FT was initially validated for ventricular function analysis^[21-27], its applicability has recently been extended to quantitative longitudinal LA strain and SR analysis^[7]. Typically, LA endocardial borders are initially traced in the 2- and 4-chamber views at the minimum atrial volume after atrial contraction^[7]. Subsequently, an automatic tracking algorithm is applied. According to STE, LA contours are divided into six segments^[20] and subsequently averaged to global strain and SR indexes using a 12-segment model (six equidistant segments in the 4 and 2-chamber views). CMR-FT benefits from high quality CMR images allowing robust contouring of the thin LA myocardium. Furthermore, CMR includes the acquisition of standardised and highly reproducible imaging planes, which is particularly important in longitudinal studies with repeated measurements^[28]. Future studies will need to address whether or not CMR-FT has better inter-study reproducibility than STE. On the other hand, low temporal resolution of CMR images might affect deformation analysis, *e.g.*, the ability to accurately quantify peak strain rates^[7]. Future evaluations will have to compare STE and CMR-

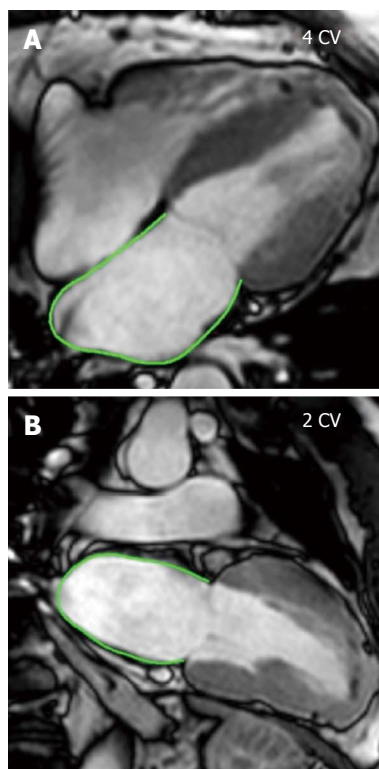


Figure 2 Cardiovascular magnetic resonance myocardial feature tracking of the left atrium in a patient with hypertrophic cardiomyopathy. Cardiovascular magnetic resonance myocardial feature tracking is performed in 4-chamber (A) and 2-chamber (B) views. Contours are based on 48 features, which are tracked throughout the cardiac cycle to generate longitudinal strain and strain rate profiles as displayed in Figure 1.

FT regarding the analysis of LA dynamics to determine whether or not results are interchangeable between modalities or one approach should be preferred over the other.

FUTURE POTENTIAL OF LA DEFORMATION QUANTIFICATION

A growing body of literature suggests to focus on the quantification of the three basic LA functions rather than on the LA volumes only: LA reservoir function has shown to closely correlate with LV filling pressures^[29] and has demonstrated to be a sensitive biomarker for the prediction of adverse cardiac events independently of other measures of cardiac dysfunction in patients with heart failure^[30]. Strong association between LA conduit function and recurrent atrial fibrillation after pulmonary vein isolation has been described^[31]. Accordingly, there has been tremendous effort to study LA dynamics with STE. Mounting evidence suggests that impaired LA strain and SR dynamics have the potential to serve as imaging biomarkers for the prognosis and risk stratification or the decision to intervene in heart failure^[32,33], hypertension^[34], coronary artery disease^[35], atrial fibrillation^[36], valvular heart disease^[20] and cardiomyopathies^[37,38] (please see reviews by Hoit^[6] and

Viera *et al.*^[17] for in depth information).

CMR-FT has been introduced more recently^[7]. However, recent studies were able to demonstrate an association of impaired LA reservoir function and the development of heart failure in the general population^[39]. Impaired reservoir function as determined by volumetric indexes, strain and SR measurements is also closely related to LV fibrosis^[40]. With respect to previous reports on the relevance of LV fibrosis^[41], LA reservoir function may also represent a promising target for risk stratification. Furthermore, initial experiences on patients with hypertrophic cardiomyopathy (HCM) and heart failure with preserved ejection fraction (HFpEF) demonstrate impaired LA reservoir and conduit function in HCM and HFpEF^[7], when compared to healthy controls. In contrast, patients with HCM exhibit increased LA booster pump function while this is decreased in HFpEF^[7]. Future studies will need to investigate whether or not this might refer to a potential compensatory mechanism in HCM, as opposed to a complete impairment of LA dynamics in HFpEF^[7]. LA CMR-FT has not been applied to patients with atrial fibrillation yet. Deteriorated image quality, which is frequently present in patients with atrial fibrillation, might negatively impact on CMR-FT quality. It remains to be investigated whether or not CMR-FT is feasible in patients with atrial fibrillation using both, conventional ECG-gated SSFP sequences or real-time CMR techniques^[42,43], which have demonstrated improved image quality in arrhythmic patients as compared to conventional ECG-gated techniques^[44].

CONCLUSION

LA physiology and pathophysiology as quantified by STE and CMR-FT carry promising clinical and prognostic implications. Future studies will need to apply LA deformation imaging to support our understanding of heart failure development and risk stratification in valvular heart disease, atrial fibrillation, hypertension, coronary artery disease and different types of cardiomyopathy.

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